

FAST FIELD-CYCLING MRI: T₁-DISPERSION FOR ENHANCED MEDICAL DIAGNOSIS

David J. Lurie, Lionel M. Broche, Gareth R. Davies, Nicholas R. Payne,
P. James Ross and Vasileios Zampetoulas

*Aberdeen Biomedical Imaging Centre, University of Aberdeen, AB25 2ZD, Scotland, UK
www.ffc-mri.org*

Fast Field-Cycling Magnetic Resonance Imaging (FFC-MRI) exploits the variation of T_1 with magnetic field strength (T_1 -dispersion), with the aim of increasing the diagnostic potential of MRI [1].

NMR relaxometry is often implemented using FFC, by switching the magnetic field rapidly between levels during the pulse sequence. In this way, a single instrument can be used to measure T_1 over a wide range of magnetic field strengths. FFC-MRI aims to obtain spatially-resolved T_1 -dispersion data, by collecting images at a range of evolution field strengths [1-3]. We have demonstrated methods for implementing relaxometry on localised regions defined on a pilot image [4]. We have also shown that FFC relaxometry can detect the formation of cross-linked fibrin protein from fibrinogen *in vitro*, in a model of the blood clotting process, via the measurement of ^{14}N - ^1H cross-relaxation phenomena [5], and we have shown that FFC-MRI can detect changes in human cartilage induced by osteoarthritis [6]. Recent work has focussed on speeding up the collection of FFC-MRI images by incorporating rapid MRI scanning methods and improved pulse sequences and algorithms [7,8].

In our lab we have built a range of FFC-MRI equipment, including two whole-body human sized scanners, operating at detection fields of 0.06 T [9] and 0.2 T [10]. The 0.06 T scanner uses a double magnet, with field-cycling being accomplished by switching on and off a resistive magnet inside the bore of a permanent magnet; this has the benefit of inherently high field stability during the detection period. The recently-completed 0.2 T FFC-MRI system uses a single resistive magnet (albeit composed of three coaxial coils) [10]. This has the advantage of increased flexibility in B_0 programming, at the expense of poorer field stability during the detection period, necessitating a higher degree of instrumental complexity.

This presentation will cover the main techniques used in FFC-MRI and will summarise current and potential bio-medical applications of the methods.

This project has received funding from the European Union's Horizon 2020 research and innovation programme under grant agreement No 668119 (project "IDentIFY").

- [1] Lurie D.J., Aime S., *et al.*, *Comptes Rendus Physique* **11**, 136-148 (2010).
- [2] Carlson J.W., Goldhaber D.M., *et al.*, *Radiology* **184**, 635-639 (1992).
- [3] Lurie D.J., 1st Symposium on Field-Cycling NMR Relaxometry, Berlin, p5, (1998).
- [4] Pine K.J., Davies G.R. and Lurie D.J., *Magn.Reson.Med.* **63**, 1698–1702 (2010).
- [5] Broche L.M., Ismail S.R., *et al.*, *Magn.Reson.Med.* **67**, 1453-1457 (2012).
- [6] Broche L.M., Ashcroft G.P and Lurie D.J., *Magn.Reson.Med.* **68**, 358-362 (2012).
- [7] Ross, P.J., Broche, L.M., and Lurie, D.J., *Magn. Reson. Med.* **73**, 1120-1124 (2015).
- [8] Broche, L.M., Ross, P.J., Pine, K.J. and Lurie, D.J., *J. Magn. Reson.*, **238**, 44-51 (2014).
- [9] Lurie D.J., Foster M.A., *et al.*, *Phys.Med.Biol.* **43**, 1877-1886 (1998).
- [10] Ross P.J., Broche L.M., *et al.*, *Proc. 25th ISMRM, Hawaii*, p2677 (2017).